

MOTIVATION

Electrocardiogram (ECG) P-waves, which represent atrial contraction of the heart, are of significant importance to cardiac health due to the high prevalence of atrial fibrillation. Two main **challenges** are associated with detecting the P-wave using machine learning tools:

Difficulty in detecting atrial electrical activity in long-term monitoring ECG recordings

Interpretation of machine learning models for application to real clinical practice

Detecting ECG P-waves using interpretable machine learning

METHODS

Autoencoders (AE). Dimensionality reduction models that compress the input data to extract relevant patterns (*encoder*) in order to reconstruct the input data to the output (*decoder*).

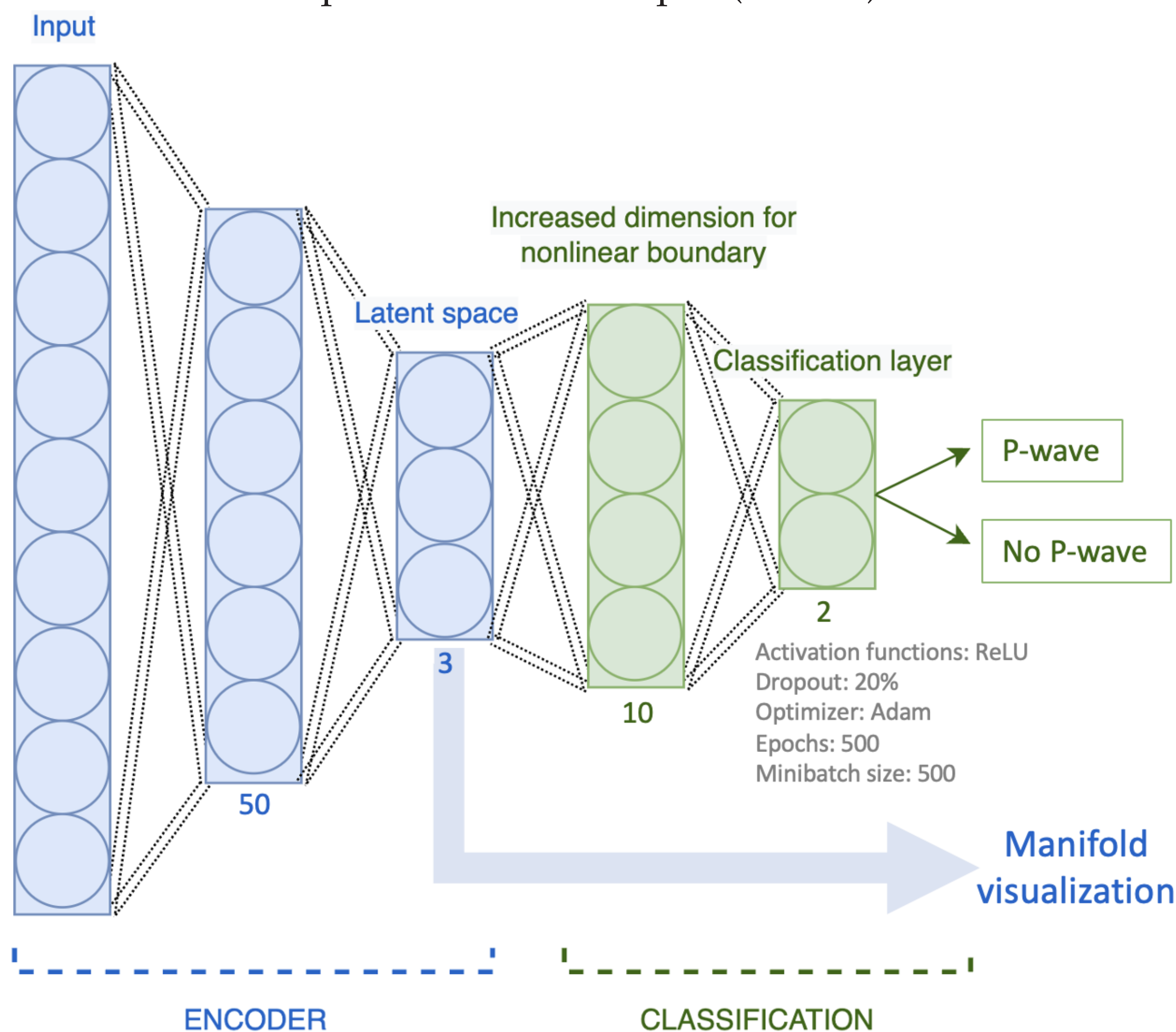


Figure 1: Neural network based on AE architecture for P-wave detection.

Based on AE architecture, a fully connected network has been created (Fig. 1), which compresses ECG data up to the *latent space* layer where the significant features are located.

Not only is it possible to perform classification on the latent space **manifolds**, but it can also **provide interpretability** to the functioning and decision making of the network.

DATABASES

Patient recordings have been segmented and labeled using a sliding window of 1-second (s), advancing in steps of 0.02-s, and a *proximity area* of 0.40-s, so that the **system can learn to work in a real situations** without prior beat delineation to detect P-waves (Fig. 2: top). Two ECG delineation databases have been used:

- **LUDB** [1]: 10-s long recordings of 200 patients have been used to train and validate the network due the availability of manual annotations. Randomly 85% of the segments to train and the remaining 15% to validate.
- **QTDB** [2]: 25 patients have been used to test the model. Only the manually labeled fragments of these 15-minutes (min) recordings have been used and segmented, approximately 1-min per patient.

Proximity area is defined as a means to obtain **balanced classes sets** for training and testing (Fig. 2: bottom).

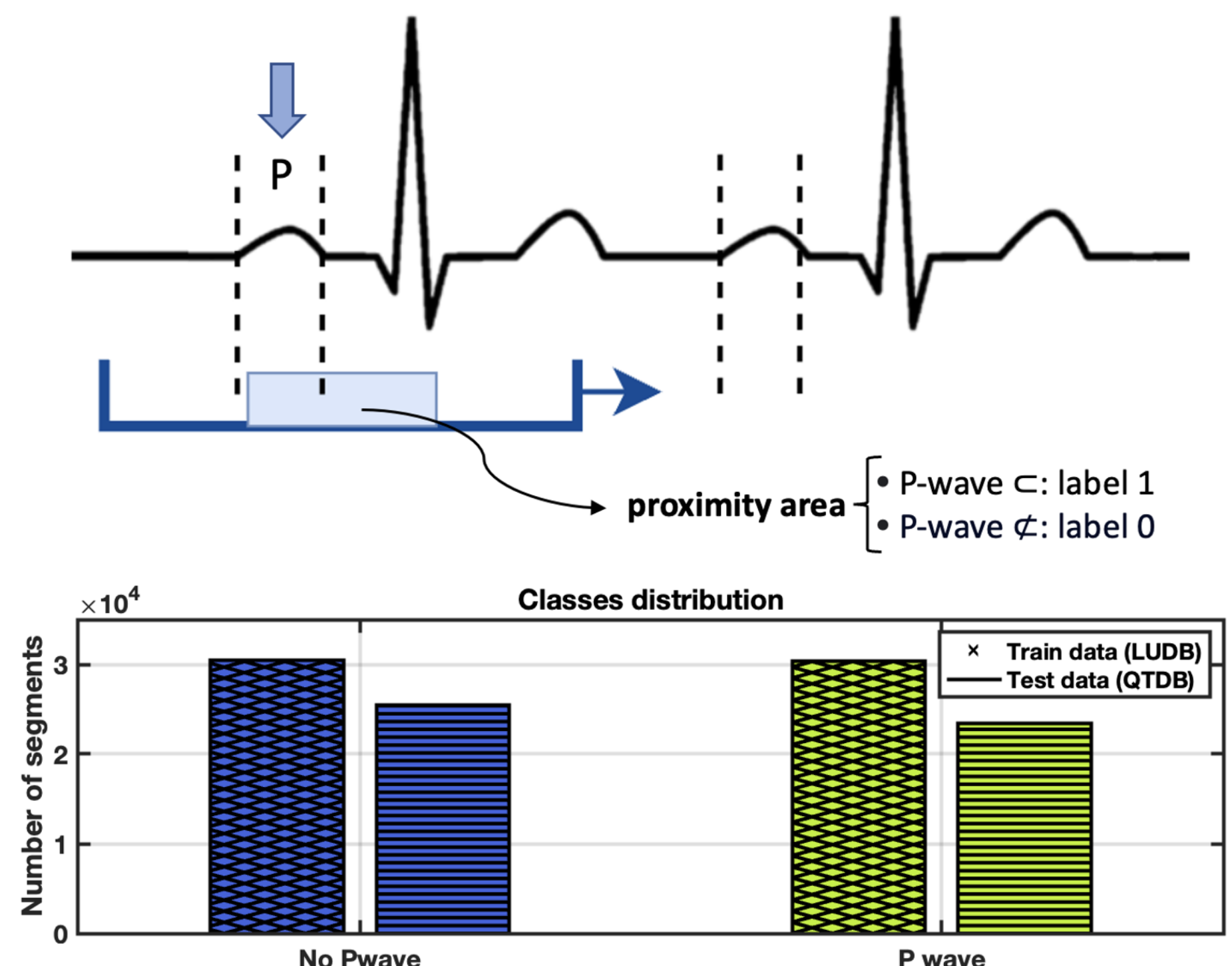


Figure 2: Recording segmentation and labeling process (top); Train-test classes distribution after segmentation (bottom).

EXPERIMENTS

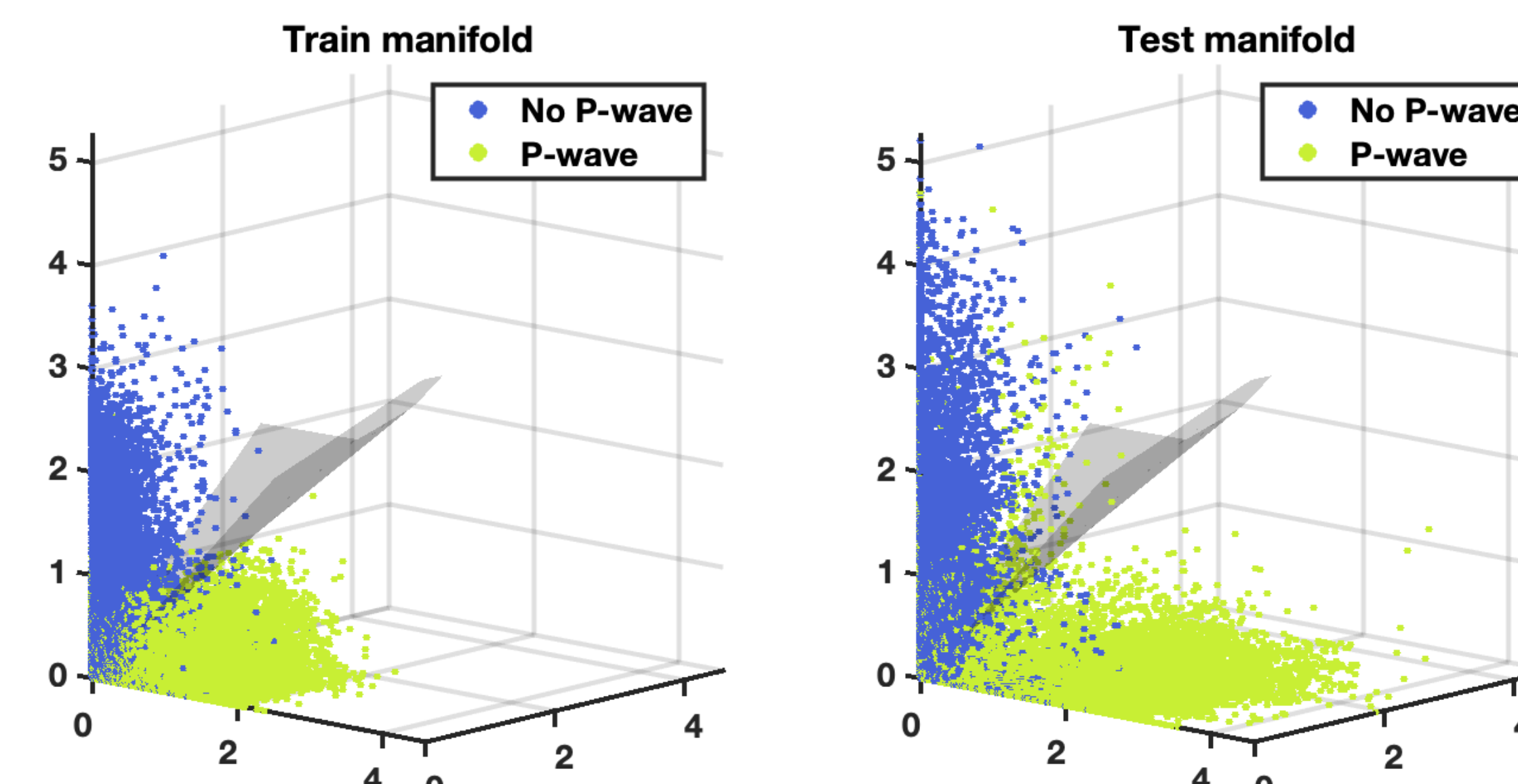


Figure 3: Train and test latent spaces manifolds with network classification boundary.

Different regions of the latent space can be **associated with each class**. Classification boundary and data projections (Fig. 3) provide a qualitative explanation of the network predictions.

The model is tested on new data consisting of real ECG fragments. The system yields **predictions close to the annotations**, although it still elicits some false positives (Fig. 4).

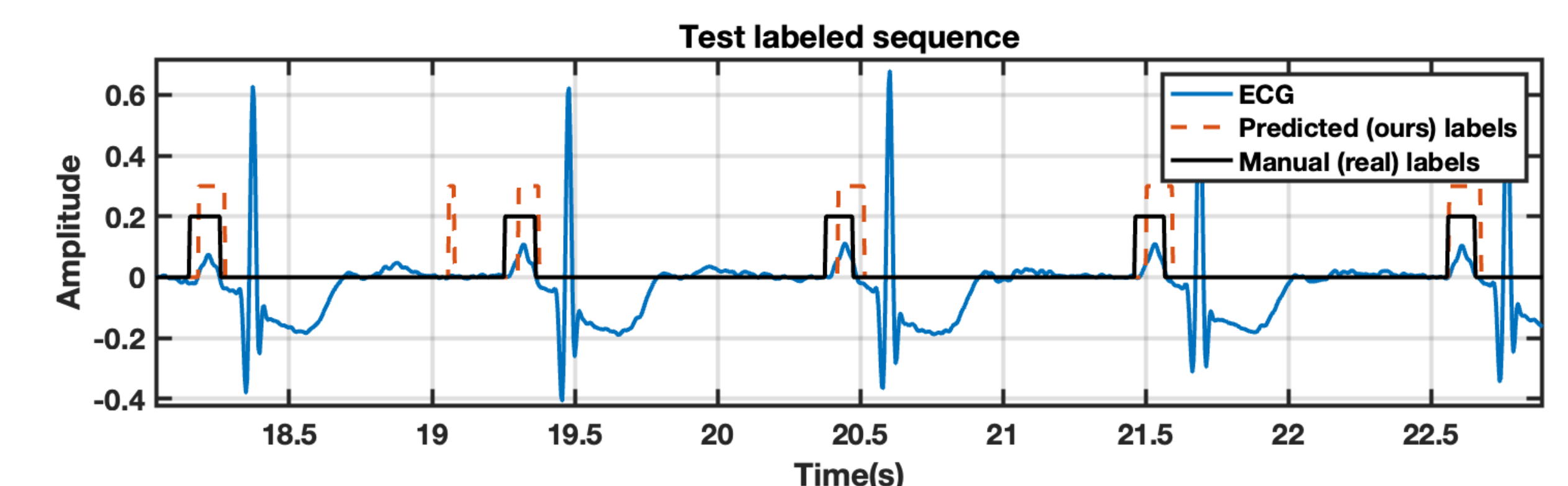


Figure 4: Test signal fragment with expert annotations and our predictions.

Table 1: Average of F1 scores of model performance after 10 simulations.

Train	Validation	Test
0.93 \pm 0.004	0.92 \pm 0.003	0.90 \pm 0.007

CONCLUSION

- Joint visual inspection of data projections in latent spaces and classification boundaries provides the opportunity to **interpret model decision making**.
- This model provides tools to increase the **confidence of medical staff** in these systems.
- Confidence improvement will enable the **application** of these systems **to real clinical practice**.

ACKNOWLEDGEMENT

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FUTURE WORK

- **Different network layouts** with convolutional or LSTM layers.
- **Extrapolate to other waves**, such as T-wave related to sudden death pathology.
- Exploring **graph learning** models for ECG waveform detection.

REFERENCES

- [1] Kalyakulina, A., Yusipov, I., Moskalenko, V., *et al.*, "Lobachevsky university electrocardiography database," *PhysioNet*, 2021.
- [2] P. Laguna, R.G. Mark, A. Goldberger, and G.B. Moody, "A Database for Evaluation of Algorithms for Measurement of QT and Other Waveform Intervals in the ECG," *Computers in Cardiology*, vol. 24, 673–676, 1997.